

# 1 Functional MRI brain state 2 occupancy in the presence of 3 cerebral small vessel disease – 4 pre-registration for a replication 5 analysis of the Hamburg City Health 6 Study

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Preprocessed data will be  
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## 11 Abstract

12 **Objective:** To replicate recent findings about the association between the extent of  
13 cerebral small vessel disease (cSVD), functional brain network dedifferentiation and  
14 cognitive impairment.

15 **Methods:** We will analyze demographic, imaging and behavioral data from the  
16 prospective population-based Hamburg City Health Study. Using a fully prespecified  
17 analysis pipeline, we will estimate discrete brain states from structural and resting-state  
18 functional magnetic resonance imaging (MRI). In a multiverse analysis we will vary brain  
19 parcellations and functional MRI confound regression strategies. Severity of cSVD will  
20 be operationalised as the volume of white matter hyperintensities of presumed  
21 vascular origin. Processing speed and executive dysfunction are quantified by the trail  
22 making test (TMT).

23 **Hypotheses:** We hypothesize a) that greater volume of supratentorial white matter

24 hyperintensities is associated with less time spent in functional MRI-derived brain  
25 states of high fractional occupancy; and b) that less time spent in these high-occupancy  
26 brain states is associated with longer time to completion in part B of the TMT.

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## 28 Introduction

29 Cerebral small vessel disease (cSVD) is an arteriopathy of the brain, associated with  
30 age and common cardiovascular risk factors (Wardlaw, C. Smith, and Dichgans, 2013).  
31 cSVD predisposes to ischemic, in particular lacunar, stroke and may lead to cognitive im-  
32 pairment and dementia (Cannistraro et al., 2019). Neuroimaging findings in cSVD reflect  
33 its underlying pathology (Wardlaw, Valdés Hernández, and Muñoz-Maniega, 2015) and  
34 include white matter hyperintensities (WMH) and lacunes of presumed vascular origin,  
35 small subcortical infarcts and microbleeds, enlarged perivascular spaces as well as brain  
36 atrophy (Wardlaw, E. E. Smith, et al., 2013). However, the extent of visible cSVD features  
37 on magnetic resonance imaging (MRI) is an imperfect predictor of the severity of clini-  
38 cal sequelae (Das et al., 2019), and our understanding of the causal mechanisms linking  
39 cSVD-associated brain damage to clinical deficits remains limited (Bos et al., 2018).

40 Recent efforts have concentrated on exploiting network aspects of the structural (Tu-  
41 ladhar, Dijk, et al., 2016; Tuladhar, Tay, et al., 2020; Lawrence, Zeestraten, et al., 2018)  
42 and functional (Dey et al., 2016; Schulz et al., 2021) organization of the brain to under-  
43 stand the relation between cSVD and clinical deficits in cognition and other domains re-  
44 liant on distributed processing. Reduced structural network efficiency has repeatedly  
45 been described as a causal factor in the development of cognitive impairment, in partic-  
46 ular executive dysfunction and reduced processing speed, in cSVD (Lawrence, Chung,  
47 et al., 2014; Shen et al., 2020; Reijmer et al., 2016; Prins et al., 2005). Findings with  
48 respect to functional connectivity results(FC), on the other hand, are more heteroge-  
49 neous ~~, perhaps due to its limited reproducibility in~~ than their SC counterparts, perhaps  
50 because FC measurements are prone to be affected by hemodynamic factors and noise,  
51 resulting in relatively low reliability, especially with resting-state scans of short duration  
52 (Laumann, Gordon, et al., 2015). This problem is exacerbated in the presence of cSVD  
53 and ~~dependence on~~ made worse by the arbitrary processing choices (Lawrence, Tozer,  
54 et al., 2018; Gesierich et al., 2020).

55 As a promising new avenue, time-varying, or dynamic, functional connectivity approaches

56 have more recently been explored in patients with subcortical ischemic vascular disease  
57 (Yin et al., 2022; Xu et al., 2021). While the study of dynamic FC measures may not  
58 solve the problem of limited reliability, especially in small populations or subjects with  
59 extensive structural brain changes, it adds another – temporal – dimension to the study of  
60 functional brain organisation, which is otherwise overlooked. Importantly, FC dynamics  
61 do not only reflect moment-to-moment fluctuations in cognitive processes but are also  
62 related to brain plasticity and homeostasis (Laumann and Snyder, 2021; Laumann, Snyder,  
63 et al., 2017), which may be impaired in cSVD.

64 In the present paper, we aim to replicate and extend the main results of (Schlemm et  
65 al., 2022); in this recent study, the authors analyzed MR imaging and clinical data from the  
66 prospective Hamburg City Health Study (HCHS, (Jagodzinski et al., 2020)) using a coacti-  
67 vation pattern approach to define discrete brain states and found associations between  
68 the WMH load, time spent in high-occupancy brain states characterized by activation  
69 or suppression of the default mode network (DMN) and ~~executive dysfunction~~cognitive  
70 impairment.

71 The fractional occupancy of a functional MRI-derived discrete brain state is a subject-specific  
72 measure of brain dynamics defined as the proportion of BOLD volumes assigned to that  
73 state relative to all BOLD volumes acquired during a resting-state scan.

74 Our primary hypothesis is that the volume of supratentorial white matter hyperinten-  
75 sities is associated with the fractional occupancy (~~defined below~~) of DMN-related brain  
76 states in a middle-aged to elderly population mildly affected by cSVD. Our second hy-  
77 pothesis is that this fractional occupancy is associated with executive dysfunction and  
78 reduced processing speed, measured as the time to complete part B of the trail making  
79 test (TMT).

80 Both hypotheses will be tested in an independent subsample of the HCHS study popu-  
81 lation using the same imaging protocols, examination procedures and analysis pipelines  
82 as in (Schlemm et al., 2022). The robustness of associations will be explored in a multi-  
83 verse approach by varying key steps in the analysis pipeline.

## 84 **Methods**

### 85 **Study population**

86 The paper will analyze data from the Hamburg City Health Study (HCHS), which is an  
87 ongoing prospective, population-based cohort study aiming to recruit a cross-sectional

Question	Hypothesis	Sampling plan	Analysis plan	Rationale for deciding the sensitivity of the test	Interpretation given different outcomes	Theory that could be shown wrong by the outcome
Is severity of cerebral small disease, quantified by the volume of supratentorial white matter hyperintensities of presumed vascular origin (WMH), associated with time spent in high-occupancy brain states, defined by resting-state functional MRI	Higher WMH volume is associated with lower average occupancy of the two highest-occupancy brain states.	Available subjects with clinical and imaging data from the the HCHS (Jagodzinski et al., 2020)	Standardized preprocessing of structural and functional MRI data • automatic quantification of WMH • co-activation pattern analysis • multivariable generalised regression analyses	Tradition	$P < 0.05 \rightarrow$ rejection of the null hypothesis of no association between cSVD and fractional occupancy; $P > 0.05 \rightarrow$ insufficient evidence to reject the null hypothesis	Functional brain dynamics are not related to subcortical ischemic vascular disease.

**Table 1.** Study Design Template

88 sample of 45 000 adult participants from the city of Hamburg, Germany (Jagodzinski et al.,  
89 2020). From the first 10 000 participants of the HCHS we will aim to include those who  
90 were documented to have received brain imaging (n=2652) and exclude those who were  
91 analyzed in our previous report (Schlemm et al., 2022) (n=988), for an expected sample  
92 size of approximately 1500 participants. The ethical review board of the Landesärztekam-  
93 mer Hamburg (State of Hamburg Chamber of Medical Practitioners) approved the HCHS  
94 (PV5131), all participants provided written informed consent.

### 95 **Demographic and clinical characterization**

96 From the study database we will extract participants' age at the time of inclusion in years,  
97 their self-reported gender sex and the number of years spent in education. During the  
98 visit at the study center, participants undergo cognitive assessment using standardized  
99 tests. We will extract from the database their performance scores in the Trail Making  
100 Test part B, measured in seconds, as an operationalization of executive function and  
101 psychomotor processing speed (Tombaugh, 2004; Arbuthnott and Frank, 2000).

### 102 **MRI acquisition and preprocessing**

103 The magnetic resonance imaging protocol for the HCHS includes structural and resting-  
104 state functional sequences. The acquisition parameters on a 3 T Siemens Skyra MRI scan-  
105 ner (Siemens, Erlangen, Germany) have been reported before (Petersen et al., 2020; Frey  
106 et al., 2021) and are given as follows:

107 For  $T_1$ -weighted anatomical images, a 3D rapid acquisition gradient-echo sequence  
108 (MPRAGE) was used with the following sequence parameters: repetition-repetition time  
109 TR = 2500 ms, echo time TE = 2.12 ms, 256 axial slices, slice thickness ST = 0.94 mm, and  
110 in-plane resolution IPR = (0.83 × 0.83) mm<sup>2</sup>.

111  $T_2$ -weighted fluid attenuated inversion recovery (FLAIR) images were acquired with  
112 the following sequence parameters: TR = 4700 ms, TE = 392 ms, 192 axial slices, ST =  
113 0.9 mm, IPR =  $(0.75 \times 0.75)$  mm<sup>2</sup>.

114 125 resting state functional MRI volumes were acquired (TR = 2500 ms; TE = 25 ms;  
115 flip angle = 90°; slices = 49; ST = 3 mm; slice gap = 0 mm; IPR =  $(2.66 \times 2.66)$  mm<sup>2</sup>). Subjects  
116 were asked to keep their eyes open and to think of nothing.

117 We will verify the presence and voxel-dimensions of expected MRI data for each par-  
118 ticipant and exclude those for whom at least one of  $T_1$ -weighted, FLAIR and resting-state  
119 MRI is missing. We will also exclude participants with a neuroradiologically confirmed  
120 space-occupying intra-axial lesion. To ensure reproducibility, no visual quality assess-  
121 ment on raw images will be performed.

122 For the remaining participants, structural and resting-state functional MRI data will  
123 be preprocessed using FreeSurfer v6.0 (<https://surfer.nmr.mgh.harvard.edu/>), and fmriPrep  
124 v20.2.6 (Esteban et al., 2019), using default parameters. Participants will be excluded if  
125 automated processing using at least one of these packages fails.

## 126 **Quantification of WMH load**

127 For our primary analysis, the extent of ischemic white matter disease will be operational-  
128 ized as the total volume of supratentorial WMHs obtained from automated segmentation  
129 using a combination of anatomical priors, BIANCA (Griffanti, Zamboni, et al., 2016) and  
130 LOCATE (Sundaresan et al., 2019), post-processed with a minimum cluster size of 30 vox-  
131 els, as described in (Schlemm et al., 2022). In an exploratory analysis, we partition voxels  
132 identified as WMH into deep and periventricular components according to their distance  
133 to the ventricular system (cut-off 10 mm, (Griffanti, Jenkinson, et al., 2018))

## 134 **Brain state estimation**

135 Output from fMRIprep will be post-processed using xcpEngine v1.2.1 to obtain de-confounded  
136 spatially averaged BOLD time series (Circic, Wolf, et al., 2017). For the primary analysis we  
137 will use the  $36p$  regression strategy and the Schaefer-400 parcellation (Schaefer et al.,  
138 2018), as in (Schlemm et al., 2022).

139 Different atlases and confound regression strategies, as implemented in xcpEngine,  
140 will be included in the exploratory multiverse analysis.

141 Co-activation pattern (CAP) analysis will be performed by first aggregating parcellated,  
142 de-confounded BOLD signals into a  $(n_{\text{parcels}} \times \sum_i n_{\text{time points},i})$  feature matrix, where  $n_{\text{time points},i}$

143 denotes the number of retained volumes for subject  $i$  after confound regression. Cluster-  
144 ing will be performed using the  $k$ -means algorithm ( $k = 5$ ) with distance measure given  
145 by 1 minus the sample Pearson correlation between points, as implemented in Matlab  
146 R2021a. We will estimate subject- and state-specific fractional occupancies, which are  
147 defined as the proportion of BOLD volumes assigned to each brain state (Vidaurre et al.,  
148 2018). The two states with the highest average occupancy will be identified as the basis  
149 for further analysis.

## 150 **Statistical analysis**

151 For demographic (age, [gendersex](#), years of education) and clinical (TMT-B) variables the  
152 number of missing records will be reported. For non-missing values, we will provide  
153 descriptive summary statistics using median and interquartile range. The proportion of  
154 men and women in the sample will be reported. [Regression modelling will be carried out  
155 as a complete-case analysis.](#)

156 As a first outcome-neutral quality check of the implementation of the MRI process-  
157 ing pipeline, brain state estimation and co-activation pattern analysis, we will compare  
158 fractional occupancies between brain states. We expect that the average fractional oc-  
159 cupancy in two high-occupancy states is higher than the average fractional occupancy in  
160 the other three states. Point estimates and 95% confidence intervals will be presented  
161 for the difference in average fractional occupancy to check this assertion.

162 For further analyses, non-zero WMH volumes will be subjected to a logarithmic trans-  
163 formation. Zero values will retain their value zero; to compensate, all models will include  
164 a binary indicator for zero WMH volume if at least one non-zero value is present.

165 To assess the primary hypothesis of a negative association between the extent of is-  
166 chemic white matter disease and time spent in high-occupancy brain states, we will per-  
167 form a fixed-dispersion beta-regression to model the logit of the conditional expectation  
168 of the average fractional occupancy of two high-occupancy states as an affine function  
169 of the logarithmized WMH load. Age and [gendersex](#) will be included as covariates. The  
170 strength of the association will be quantified as an odds ratio per interquartile ratio of the  
171 WMH burden distribution and accompanied by a 95% confidence interval. Significance  
172 testing of the null hypothesis of no association will be conducted at the conventional  
173 significance level of 0.05. Estimation and testing will be carried out using the 'betareg'  
174 package v3.1.4 in R v4.2.1.

175 To assess the secondary hypothesis of an association between time spent in high-

176 occupancy brain states and executive dysfunction, we will perform a generalized linear  
177 regression with a Gamma response distribution to model the logarithm of the conditional  
178 expected completion time in part B of the TMT as an affine function of the average frac-  
179 tional occupancy of two high-occupancy states. Age, ~~gender~~sex, years of education and  
180 logarithmized WMH load will be included as covariates. The strength of the association  
181 will be quantified as a multiplicative factor per percentage point and accompanied by a  
182 95% confidence interval. Significance testing of the null hypothesis of no association will  
183 be conducted at the conventional significance level of 0.05. Estimation and testing will  
184 be carried out using the glm function included in the 'stats' package from R v4.2.1.

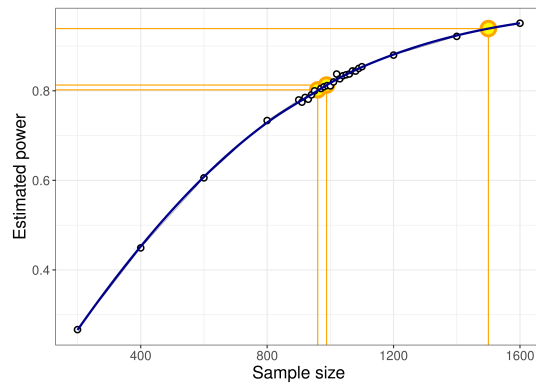
185 Sample size calculation is based on ~~the data presented in~~, ~~where an odds ratio of was~~  
186 ~~reported as the primary~~ an effect size on the odds ratio scale of 0.95, corresponding to  
187 an absolute difference in the probability of occupying a DMN-related brain state between  
188 the first and third WMH-load quartile of 1.3 percentage points, and between the 5% and  
189 95% percentile of 3.1 percentage points. Approximating half the difference in fractional  
190 occupancy of DMN-related states between different task demands (rest vs n-back) in  
191 healthy subjects, which was estimated to lie between 6 and 7 percentage points (Corn-  
192 blath et al., 2020), this value represent a plausible choice for the smallest effect size of  
193 interest theoretical and practical interest. It also equals the effect size estimated based  
194 on the data presented in (Schlemm et al., 2022).

195 We used simple bootstrapping to create 10 000 hypothetical datasets of size 200, 400,  
196 600, 800, 900, 910, ..., 1100, 1200, 1400, 1500, 1600. Each dataset was subjected to the esti-  
197 mation procedure described above. For each sample size, the proportion of datasets in  
198 which the primary null hypothesis of no association between fractional occupancy and  
199 WMH load could be rejected at  $\alpha = 0.05$  was computed and is recorded as a power curve  
200 in Figure 1.

201 It is seen that a sample size of 960 would allow replication of the reported effect with  
202 a power of 80.2 %. We anticipate a sample size of 1500, which yields a power of 93.9 %.

## 203 **Multiverse analysis**

204 Both in (Schlemm et al., 2022) and for our primary replication analysis we made cer-  
205 tain analytical choices in the ~~operationalisation~~ operationalization of brain states and  
206 ischemic white matter disease, namely the use of the 36p confound regression strat-  
207 egy, the Schaefer-400 parcellation and a BIANCA/LOCATE-based WMH segmentation al-  
208 gorithm. ~~If the hypothesized~~ The robustness of the association between WMH burden



**Figure 1.** Estimated power for different sample sizes is obtained as the proportion of synthetic data sets in which the null hypothesis of no association between WMH volume and time spent in high-occupancy brain states can be rejected at the  $\alpha = 0.05$  significance level. Proportions are based on a total of 10 000 synthetic data sets obtained by bootstrapping the data presented in (Schlemm et al., 2022). Highlighted in orange are the smallest sample size ensuring a power of at least 80 % ( $n = 960$ ), the sample size of the pilot data ( $n = 988$ , post-hoc power 81.3 %), and the expected sample size for this replication study ( $n = 1500$ , a-priori power 93.9 %).

Name of the atlas	#parcels	Reference	Design	Reference
Desikan-Killiany	86	Desikan et al., 2006	24p	Friston et al., 1996
AAL	116	Tzourio-Mazoyer et al., 2002	24p + GSR	Macey et al., 2004
Harvard-Oxford	112	Makris et al., 2006	36p	Satterthwaite et al., 2013
glasser360	360	Glasser et al., 2016	26p-36p + spike regression	Cox, 1996
gordon333	333	Gordon et al., 2016	36p + despiking	Satterthwaite et al., 2013
power264	264	Power, Cohen, et al., 2011	36p + scrubbing	Power, Mitra, et al., 2014
schaefer{N}	100	Schaefer et al., 2018	aCompCor	Muschelli et al., 2014
	200		tCompCor	Behzadi et al., 2007
	400		AROMA	Pruim et al., 2015

AAL: Automatic Anatomical Labelling

**(a)** Parcellations

GSR: Global signal regression, AROMA: ~~bla~~  
Automatic Removal of Motion Artifacts

**(b)** Confound regression strategies, adapted from (Circ, Wolf, et al., 2017)

**Table 2.** Multiverse analysis, implemented using xcpEngine (Circ, Rosen, et al., 2018)

209 and time spent in high-occupancy states ~~can be replicated using these primary analytical~~  
 210 ~~choices, its robustness~~ with regard to other choices will be explored in a multiverse anal-  
 211 ysis (Steenen et al., 2016). Specifically, in an exploratory analysis, we will estimate brain  
 212 states from BOLD time series processed according to a variety of established confound  
 213 regression strategies and aggregated over different cortical brain parcellations (Table 2,  
 214 Circ, Rosen, et al., 2018; Circ, Wolf, et al., 2017). Extent of cSVD will additionally be quan-  
 215 tified by the volume of deep and periventricular white matter hyperintensities.

216 For each combination of analytical choice of confound regression strategy, parcella-  
 217 tion and subdivision of white matter lesion load ( $9 \times 9 \times 3 = 243$  scenarios in total) we will  
 218 quantify the association between WMH load and average time spent in high-occupancy  
 219 brain states using odds ratio and 95 % confidence intervals as described above.

220 No hypothesis testing and ~~, therefore, no adjustment for multiple testing,~~ will be



221 carried out in these ~~non-primary analyses.~~ multiverse analyses. They rather serve to  
222 inform about the robustness of the outcome of the test of the primary hypothesis. Any  
223 substantial conclusions about the association between severity of cerebral small pathology  
224 and time spent in high-occupancy brain states, as stated in the Scientific Question in  
225 Table 1, will be drawn from the primary analysis using pre-specified methodological choices.

226

## 227 ~~Exploratory~~ **Further exploratory analysis**

228 In previous work, two high-occupancy brain states were related to the default-mode net-  
229 work (Cornblath et al., 2020). We will further explore this relation by computing, for each  
230 individual brain state, the cosine similarity of the positive and negative activations of  
231 the cluster's centroid with a set of a-priori defined functional 'communities' or networks  
232 (Schaefer et al., 2018; Yeo et al., 2011). Results will be thus visualized as spider plots for  
233 the Schaefer, Gordon and Power ~~atlases~~ atlases.

234 In further exploratory analyses we plan to describe the associations between brain  
235 state dynamics and other measures of cognitive ability, such as memory and language.

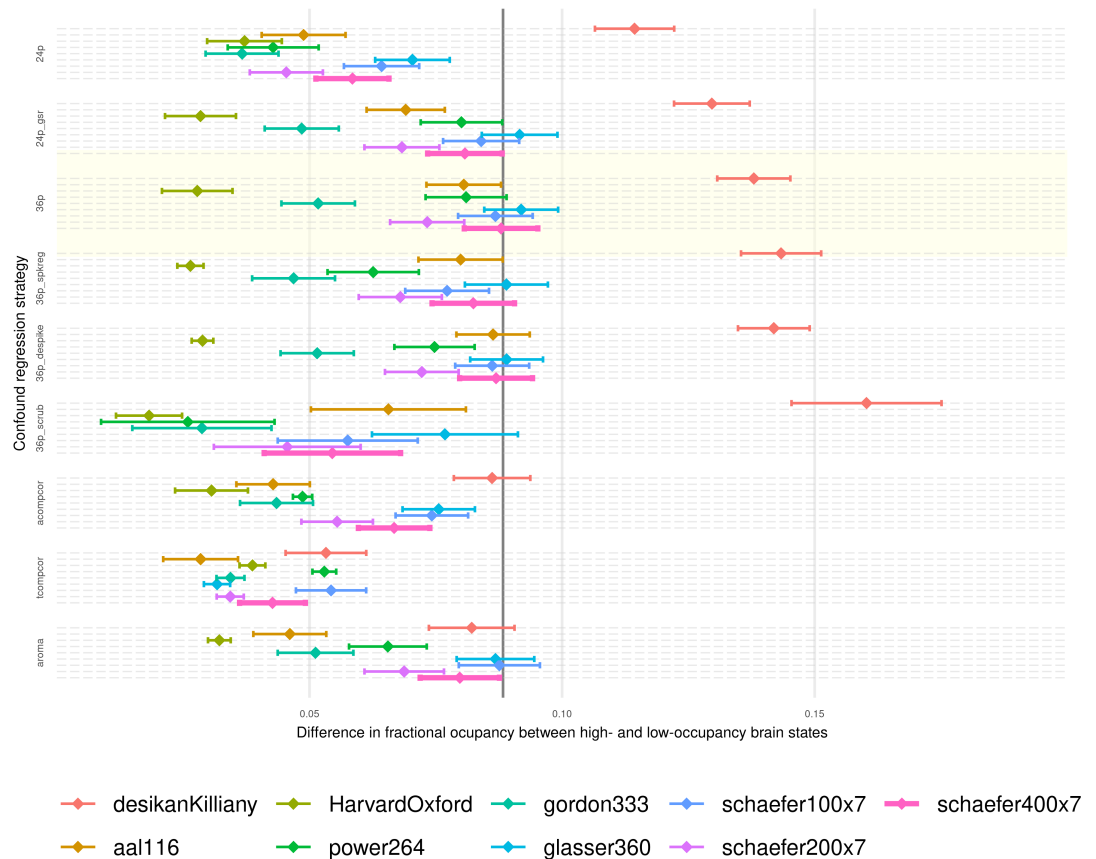
## 236 **Code and pilot data**

237 Summary data from the first 1000 imaging data points of the HCHS have been published  
238 with (Schlemm et al., 2022) and form the basis for the hypotheses tested in this replication  
239 study. We have implemented our prespecified analysis pipeline described above in R  
240 and Matlab, and applied it to this previous sample. Data, code and results have been  
241 stored on GitHub ([https://github.com/csi-hamburg/HCHS\\_brain\\_states\\_RR](https://github.com/csi-hamburg/HCHS_brain_states_RR)) und preserved  
242 on Zenodo.

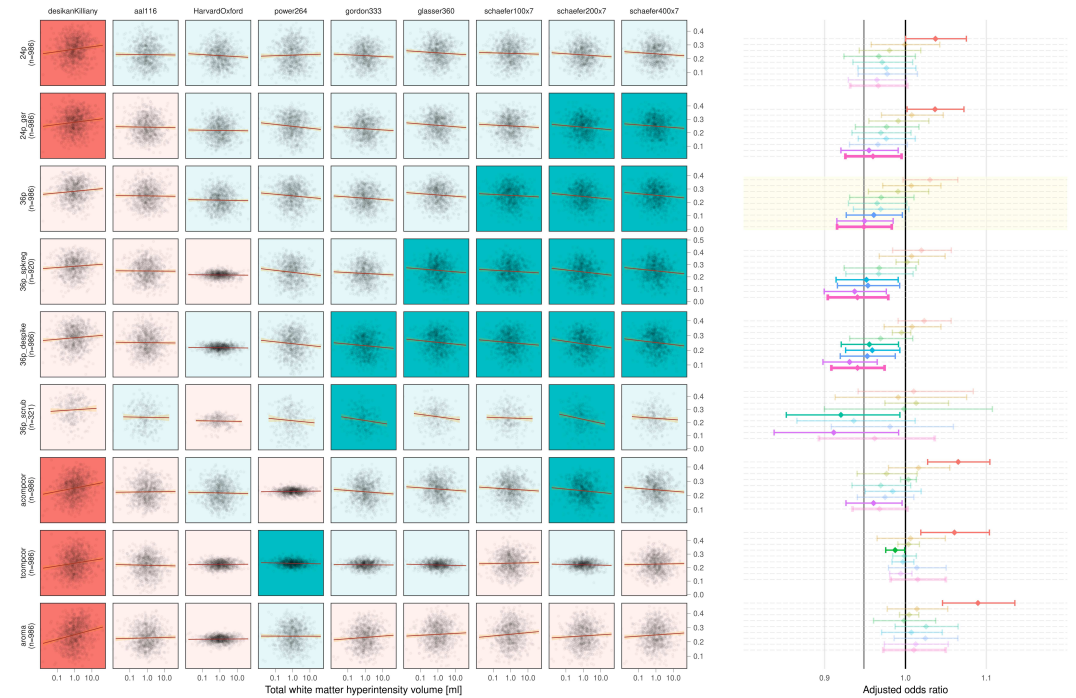
243 Thus re-analysing data from 988 subjects, the separation between two high-occupancy  
244 and three low-occupancy brain states could be reproduced for all combinations of brain  
245 parcellation and confound regression strategies (Figure 2).

246 In a multiverse analysis, the main finding was somewhat robust with respect to these  
247 choices: a statistically significant negative association between WMH load and time spent  
248 in high-occupancy states was observed in 18/81 scenarios, with 5/81 statistically signifi-  
249 cant positive associations occurring with the Desikan–Killiany parcellation only (Figure 3).

250 The secondary finding of an association between greater TMT-B times and lower frac-  
251 tional occupancy was similarly robust with 12/81 statistically significant negative and no



**Figure 2.** Point estimates (dots) and 95 % confidence intervals (line segments) for the mean difference in fractional occupancy between high- and low occupancy states are shown for different confound regression strategies (groups along the vertical axis) and brain parcellations (color). The difference in FO for a particular choice of regression strategy and brain parcellation is nominally statistically significantly different from zero at a significance level of 5% if the corresponding interval does not contain zero. Hence, the FO difference is significant for *all* processing choices, reflecting the separation between high- und low-occupancy states. The primary choices (36p and schaefer400) are highlighted by a yellow box and thick pink line, respectively. The effect size reported in (Schlemm et al., 2022) is indicated by a vertical line at 0.08830623.



**Figure 3.** On the left, scatter plots of average fractional occupancies in high-occupancy states against WMH volume on a logarithmic scale (base 10 for easier visualization) for different combinations of confound regression strategies and brain parcellations. Linear regression lines indicate the direction of the unadjusted association between  $\log(\text{WMH})$  and occupancy. Background color of individual panels indicates the direction of the association after adjustment for age, sex and zero WMH volume (green, negative; red, positive). A pale background indicates that the association between  $\log(\text{WMH})$  and average occupancy is not statistically different from zero. On the right, the same information is shown using point estimates and 95 % confidence intervals for the adjusted odds ratio of the association.

252 statistically significant positive associations.

## 253 **Timeline and access to data**


254 At the time of planning of this study, all demographic, clinical and imaging data used in  
255 this analysis have been collected by the HCHS and are held in the central trial database.

256 Quality checks for non-imaging variables have been performed centrally. WMH segmen-  
257 tation based on structural MRI data of the first 10 000 participants of the HCHS has been  
258 performed previously using the BIANCA/LOCATE approach (Rimmele et al., 2022) and re-

259 sults are included in this preregistration ([./derivatives/WMH/cSVD\\_all.csv](#), [./derivatives/WMH/cS](#)

260 Functional MRI data and clinical measures of executive dysfunction (TMT-B scores) have  
261 not been analyzed by the author. Analysis of the data will begin immediately after acceptance-  
262 in-principle of the stage 1 submission of the registered report is obtained. Submission  
263 of the full manuscript (stage 2) is planned two months later.

## 264 **Acknowledgment**

265 This preprint was created using the LaPreprint template ([https://github.com/roaldarbol/](https://github.com/roaldarbol/lapreprint)  
266 [lapreprint](#)) by Mikkel Roald-Arbøl .

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