

1 Functional MRI brain state 2 occupancy in the presence of 3 cerebral small vessel disease – a 4 pre-registered replication analysis of 5 the Hamburg City Health Study

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Preprocessed data is
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19 Abstract

20 **Objective:** To replicate recent findings on the association between the extent of
21 cerebral small vessel disease (cSVD), functional brain network dedifferentiation, and
22 cognitive impairment.

23 **Methods:** We analyzed demographic, imaging, and behavioral data from the

24 prospective population-based Hamburg City Health Study. Using a fully prespecified
25 analysis pipeline, we estimated discrete brain states from structural and resting-state
26 functional magnetic resonance imaging (MRI). In a multiverse analysis, we varied brain
27 parcellations and functional MRI confound regression strategies. The severity of cSVD
28 was operationalized as the volume of white matter hyperintensities of presumed
29 vascular origin. Processing speed and executive dysfunction were quantified using the
30 Trail Making Test (TMT).

31 **Hypotheses:** We hypothesized a) that a greater volume of supratentorial white matter
32 hyperintensities would be associated with less time spent in functional MRI-derived
33 brain states of high fractional occupancy; and b) that less time spent in these
34 high-occupancy brain states is associated with a longer time to completion in part B of
35 the TMT.

36 **Results:** High-occupancy brain states were characterized by activation or suppression
37 of the default mode network. Every 5.1-fold increase in WMH volume was associated
38 with a 0.94-fold reduction in the odds of occupying DMN-related brain states (P
39 5.01×10^{-8}). Every 5 % increase in time spent in high-occupancy brain states was
40 associated with a 0.98-fold reduction in the TMT-B completion time (P 0.0116). Findings
41 were robust across most brain parcellations and confound regression strategies.

42 **Conclusion:** We successfully replicated previous findings on the association between
43 cSVD, functional brain occupancy, and cognition in an independent sample. The data
44 provide further evidence for a functional network dedifferentiation hypothesis of
45 cSVD-related cognitive impairment. Further research is required to elucidate the
46 mechanisms underlying these associations.

47

48 Introduction

49 Cerebral small vessel disease (cSVD) is an arteriopathy of the brain associated with age
50 and common cardiovascular risk factors (Wardlaw, C. Smith, and Dichgans, 2013). cSVD
51 predisposes patients to ischemic stroke (in particular lacunar stroke) and may lead to
52 cognitive impairment and dementia (Cannistraro et al., 2019). Neuroimaging findings in
53 cSVD reflect its underlying pathology (Wardlaw, Valdés Hernández, and Muñoz-Maniega,
54 2015) and include white matter hyperintensities (WMH), lacunes of presumed vascular
55 origin, small subcortical infarcts and microbleeds, enlarged perivascular spaces as well

56 as brain atrophy (Wardlaw, E. E. Smith, et al., 2013). However, the extent of visible cSVD
57 features on magnetic resonance imaging (MRI) is an imperfect predictor of the severity
58 of clinical sequelae (Das et al., 2019) and our understanding of the causal mechanisms
59 linking cSVD-associated brain damage to clinical deficits remains limited (Bos et al., 2018).

60 Recent efforts have focused on exploiting network aspects of the structural (Tuladhar,
61 Dijk, et al., 2016; Tuladhar, Tay, et al., 2020; Lawrence, Zeestraten, et al., 2018) and func-
62 tional (Dey et al., 2016; Schulz et al., 2021) organization of the brain to understand the
63 relationship between cSVD and clinical deficits in cognition and other domains that rely
64 on distributed processing. Reduced structural network efficiency has repeatedly been
65 described as a causal factor in the development of cognitive impairment, particularly
66 executive dysfunction and reduced processing speed in cSVD (Lawrence, Chung, et al.,
67 2014; Shen et al., 2020; Reijmer et al., 2016; Prins et al., 2005). Findings with respect
68 to functional connectivity (FC), however, are more heterogeneous than their SC counter-
69 parts, perhaps because FC measurements are prone to be affected by hemodynamic
70 factors and noise, resulting in relatively low reliability, especially with resting-state scans
71 of short duration (Laumann, Gordon, et al., 2015). This problem is exacerbated in the
72 presence of cSVD and worsened by arbitrary processing choices (Lawrence, Tozer, et al.,
73 2018; Gesierich et al., 2020).

74 As a promising new avenue, time-varying, or dynamic, functional connectivity approaches
75 have recently been explored in patients with subcortical ischemic vascular disease (Yin
76 et al., 2022; Xu et al., 2021). Although the study of dynamic FC measures may not solve
77 the problem of limited reliability, especially in small populations or [subjects-participants](#)
78 with extensive structural brain changes, it adds another – temporal – dimension to the
79 study of functional brain organization, which is otherwise overlooked. Importantly, FC dy-
80 namics not only reflect moment-to-moment fluctuations in cognitive processes, but are
81 also related to brain plasticity and homeostasis (Laumann and Snyder, 2021; Laumann,
82 Snyder, et al., 2017), which may be impaired in cSVD.

83 In the present paper, we aimed to replicate and extend the main results of (Schlemm
84 et al., 2022). In this recent study, the authors analyzed MR imaging and clinical data from
85 the prospective Hamburg City Health Study (HCHS, (Jagodzinski et al., 2020)) using a coac-
86 tivation pattern approach to define discrete brain states and found associations between
87 the WMH load, time spent in high-occupancy brain states characterized by activation or
88 suppression of the default mode network (DMN), and cognitive impairment. Specifically,

89 every 4.7-fold increase in WMH volume was associated with a 0.95-fold reduction in the
90 odds of occupying a DMN-related brain state; every 2.5 seconds (i.e., one repetition time)
91 not spent in one of those states was associated with a 1.06-fold increase in TMT-B com-
92 pletion times.

93 The fractional occupancy of a functional MRI-derived discrete brain state is a **subject-specific**
94 participant-specific measure of brain dynamics and is defined as the proportion of BOLD
95 volumes assigned to that state relative to all BOLD volumes acquired during a resting-
96 state scan.

97 Our primary hypothesis for the present work was that the volume of supratentorial
98 white matter hyperintensities is associated with fractional occupancy of DMN-related
99 brain states in a middle-aged to elderly population mildly affected by cSVD. Our sec-
100 ondary hypothesis was that fractional occupancy is associated with executive dysfunc-
101 tion and reduced processing speed, measured as the time to complete part B of the Trail
102 Making Test (TMT).

103 Both hypotheses were tested in an independent subsample of the HCHS study popu-
104 lation using the same imaging protocols, examination procedures, and analysis pipelines
105 as those in (Schlemm et al., 2022). The robustness of the associations was explored using
106 a multiverse approach by varying key steps in the analysis pipeline.

107 **Methods**

108 **Study population**

109 This study analyzed data from the Hamburg City Health Study (HCHS), an ongoing prospec-
110 tive, population-based cohort study aiming to recruit a cross-sectional sample of 45 000
111 adult participants from the city of Hamburg, Germany (Jagodzinski et al., 2020). From
112 the first 10 000 participants of the HCHS, we planned to include those who were docu-
113 mented to have received brain imaging (n=2648) and exclude those who were analyzed
114 in our previous report (Schlemm et al., 2022) (n=970). The ethical review board of the
115 Landesärztekammer Hamburg (State of Hamburg Chamber of Medical Practitioners) ap-
116 proved the HCHS (PV5131), and all participants provided written informed consent.

117 **Demographic and clinical characterization**

118 From the study database, we extracted the participants' age at the time of inclusion in
119 years, their sex, and the number of years spent in education. During the visit to the study

120 center, participants underwent cognitive assessment using standardized tests. From the
121 database, we extracted their performance scores on the Trail Making Test part B, mea-
122 sured in seconds, as an operationalization of executive function and psychomotor pro-
123 cessing speed (Tombaugh, 2004; Arbuthnott and Frank, 2000). For descriptive purposes,
124 we also extracted data on past medical history and reported the proportion of partici-
125 pants with a previous diagnosis of dementia.

126 **MRI acquisition and preprocessing**

127 The magnetic resonance imaging protocol for the HCHS includes structural and resting-
128 state functional sequences. The acquisition parameters for a 3 T Siemens Skyra MRI scan-
129 ner (Siemens, Erlangen, Germany) have been previously reported (Petersen et al., 2020;
130 Frey et al., 2021) and are given as follows:

131 For T_1 -weighted anatomical images, a 3D rapid acquisition gradient-echo sequence
132 (MPRAGE) was used with the following sequence parameters: repetition time TR = 2500 ms,
133 echo time TE = 2.12 ms, 256 axial slices, slice thickness ST = 0.94 mm, and in-plane resolu-
134 tion IPR = (0.83×0.83) mm².

135 T_2 -weighted fluid attenuated inversion recovery (FLAIR) images were acquired with
136 the following sequence parameters: TR = 4700 ms, TE = 392 ms, 192 axial slices, ST =
137 0.9 mm, IPR = (0.75×0.75) mm².

138 125 resting state functional MRI volumes were acquired (TR = 2500 ms; TE = 25 ms;
139 flip angle = 90°; slices = 49; ST = 3 mm; slice gap = 0 mm; IPR = (2.66×2.66) mm²). The
140 ~~subjects~~participants were asked to keep their eyes open and to think of nothing.

141 We verified the presence and voxel dimensions of expected MRI data for each par-
142 ticipant and excluded those for whom at least one of T_1 -weighted, FLAIR, and resting-
143 state MRI was missing. We also excluded participants with neuroradiologically confirmed
144 space-occupying intra-axial lesion. To ensure reproducibility, no visual quality assess-
145 ment of raw images was performed.

146 For the remaining participants, structural and resting-state functional MRI data was
147 preprocessed using FreeSurfer v6.0 (<https://surfer.nmr.mgh.harvard.edu/>), and fmriPrep
148 v20.2.6 (Esteban et al., 2019), using default parameters. Participants were excluded if
149 automated processing using at least one of these packages failed.

150 **Quantification of WMH load**

151 For our primary analysis, the extent of ischemic white matter disease was operational-
152 ized as the total volume of supratentorial WMHs obtained from automated segmentation
153 using a combination of anatomical priors, BIANCA (Griffanti, Zamboni, et al., 2016), and
154 LOCATE (Sundaresan et al., 2019), post-processed with a minimum cluster size of 30 vox-
155 els, as described in (Schlemm et al., 2022). In an exploratory analysis, we partitioned
156 voxels identified as WMH into deep and periventricular components according to their
157 distance to the ventricular system (cut-off 10 mm, (Griffanti, Jenkinson, et al., 2018))

158 **Brain state estimation**

159 The output from fMRIPrep was post-processed using xcpEngine v1.2.3 to obtain de-confounded
160 spatially averaged BOLD time series (Ciric, Wolf, et al., 2017). For the primary analysis, we
161 used the $36p$ regression strategy and the Schaefer-400 parcellation (Schaefer et al., 2018),
162 as in (Schlemm et al., 2022).

163 Different atlases and confound regression strategies, as implemented in xcpEngine,
164 were included in an exploratory multiverse analysis.

165 Co-activation pattern (CAP) analysis was performed by first aggregating parcellated,
166 de-confounded BOLD signals into a $(n_{\text{parcels}} \times \sum_i n_{\text{time points},i})$ feature matrix, where $n_{\text{time points},i}$
167 denotes the number of retained volumes for [subject-participant \$i\$](#) after confound regres-
168 sion. Clustering was performed using the k -means algorithm ($k = 5$) with a distance mea-
169 sure given by 1 minus the sample Pearson correlation between points, as implemented
170 in Matlab R2021a. We estimated the [subject-participant-](#) and state-specific fractional oc-
171 cupancies, which are defined as the proportion of BOLD volumes assigned to each brain
172 state (Vidaurre et al., 2018). The two states with the highest average occupancies were
173 identified as the basis for further analysis.

174 **Statistical analysis**

175 For demographic (age, sex, and years of education) and clinical (TMT-B) variables, the
176 number of missing items is reported. For non-missing values, we provide descriptive
177 summary statistics using median and interquartile range. The proportions of men and
178 women in the sample are reported. Since we expected based on our pilot data (Schlemm
179 et al., 2022) that the proportion of missing data would be small, primary regression mod-
180 elling was carried out as a complete-case analysis.

181 As an outcome-neutral quality check of the implementation of the MRI processing
182 pipeline, brain state estimation, and co-activation pattern analysis, we compared frac-
183 tional occupancies between brain states. We expected that the average fractional oc-
184 cupancy in the two high-occupancy states would be higher than the average fractional
185 occupancy in the other three states. Point estimates and 95% confidence intervals are
186 presented for the difference in average fractional occupancy to verify this assertion.

187 For further analyses, non-zero WMH volumes were subjected to logarithmic transfor-
188 mation. Zero values retained their value of zero; to compensate, all models included a
189 binary indicator for zero WMH volume if at least one non-zero WMH value was present.

190 To assess the primary hypothesis of a negative association between the extent of
191 ischemic white matter disease and time spent in high-occupancy brain states, we per-
192 formed a fixed-dispersion Beta regression to model the logit of the conditional expect-
193 tation of the average fractional occupancy of two high-occupancy states as an affine
194 function of the logarithmized WMH load. Age and sex were included as covariates. The
195 strength of the association was quantified as the odds ratio per interquartile ratio of the
196 WMH burden distribution, and is accompanied by a 95% confidence interval. Significance
197 testing of the null hypothesis of no association was conducted at the conventional signif-
198 icance level of 0.05. Estimation and testing were carried out using the 'betareg' package
199 v3.1.4 in R v4.2.1.

200 To assess the secondary hypothesis of an association between time spent in high-
201 occupancy brain states and executive dysfunction, we performed a generalized linear
202 regression with a Gamma response distribution to model the logarithm of the condi-
203 tional expected completion time in part B of the TMT as an affine function of the average
204 fractional occupancy of two high-occupancy states. Age, sex, years of education, and
205 logarithmized WMH load were included as covariates. The strength of the association
206 was quantified as a multiplicative factor per percentage point and accompanied by a
207 95% confidence interval. Significance testing of the null hypothesis of no association was
208 conducted at the conventional significance level of 0.05. Estimation and testing were
209 performed using the glm function included in the 'stats' package from R v4.2.1.

210 **Pre-registered analyses**

211 The analysis plan was ~~pre-registered~~ [pre-registered](https://osf.io/fcqmb) on June 27 2023 at [https://osf.io/](https://osf.io/fcqmb)
212 [fcqmb](https://osf.io/fcqmb). The sample size calculation was based on an effect size on the odds ratio scale of
213 0.95, corresponding to an absolute difference in the probability of occupying a DMN-

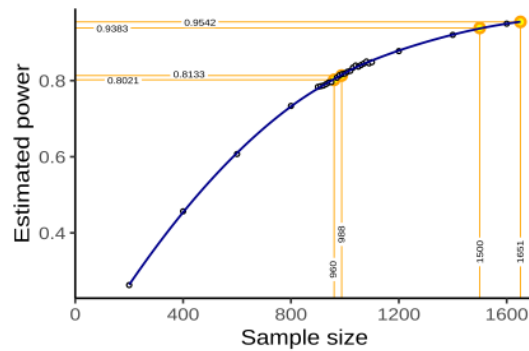


Figure 1 | Sample size and power estimation. A-priori estimated power for different sample sizes was obtained as the proportion of synthetic data sets in which the null hypothesis of no association between WMH volume and time spent in high-occupancy brain states can be rejected at the $\alpha = 0.05$ significance level. Proportions are based on a total of 10 000 synthetic data sets obtained by bootstrapping the data presented in (Schlemm et al., 2022). Highlighted in orange are the smallest sample size ensuring a power of at least 80 % ($n = 960$), the sample size of the pilot data ($n = 988$, post-hoc power 81.3 %), the expected sample size for this replication study ($n = 1500$, a-priori power 93.9 %), and the achieved sample size ($n = 1651$, a-priori power 95.4 %).

214 related brain state between the first and third WMH-load quartile of 1.3 percentage
 215 points, and between the 5% and 95% percentile of 3.1 percentage points. Approximat-
 216 ing half the difference in fractional occupancy of DMN-related states between different
 217 task demands (rest vs n-back) in healthy [subjects](#)[participants](#), which was estimated to
 218 lie between 6 and 7 percentage points (Cornblath et al., 2020), this value represented a
 219 plausible choice for the smallest effect size of theoretical and practical interest. It also
 220 equals the estimated effect size based on the data presented in (Schlemm et al., 2022).

221 Simple bootstrapping was used to create 10 000 hypothetical datasets of size 200, 400,
 222 600, 800, 900, 910, ..., 1090, 1100, 1200, 1400, 1500, and 1600. Each dataset was then sub-
 223 jected to the estimation procedure described above. For each sample size, the propor-
 224 tion of datasets in which the primary null hypothesis of no association between fractional
 225 occupancy and WMH load could be rejected at $\alpha = 0.05$ was computed and recorded as
 226 a power curve in Figure 1.

227 A sample size of 960 would have allowed the replication of the reported effect with a
 228 power of 80.2%. We had anticipated a sample size of 1500, which would have yielded a
 229 power of 93.9%.

230 Multiverse analysis

231 In both (Schlemm et al., 2022) and our primary replication analysis, we made certain ana-
 232 lytical choices in the operationalization of brain states and ischemic white matter disease,
 233 namely the use of the 36p confound regression strategy, the Schaefer-400 parcellation,

234 and a BIANCA/LOCATE-based WMH segmentation algorithm. The robustness of the as-
235 sociation between WMH burden and time spent in high-occupancy states with regard to
236 other choices was explored in a multiverse analysis (Steenen et al., 2016). Specifically, in
237 an exploratory analysis, we estimated brain states from BOLD time series processed ac-
238 cording to a variety of established confound regression strategies and aggregated over
239 different cortical brain parcellations (Table 2, Ciric, Rosen, et al., 2018; Ciric, Wolf, et al.,
240 2017). The extent of cSVD was additionally quantified by the volume of deep and periven-
241 tricular white matter hyperintensities.

242 For each combination of analytical choice of confound regression strategy, parcella-
243 tion, and subdivision of white matter lesion load ($9 \times 9 \times 3 = 243$ scenarios in total), we
244 quantified the association between WMH load and average time spent in high-occupancy
245 brain states using odds ratios and 95 % confidence intervals as described above.

246 No hypothesis testing was performed for these multiverse analyses. Rather, they
247 serve to inform about the robustness of the outcome of the test of the primary hypoth-
248 esis. Any substantial conclusions about the association between the severity of cerebral
249 small vessel pathology and the time spent in high-occupancy brain states were drawn
250 from the primary analysis using pre-specified methodological choices, as stated in the
251 Scientific Question in Table 1.

252 **Further exploratory analysis**

253 In previous work, two high-occupancy brain states have been related to the default mode
254 network (Cornblath et al., 2020). We further explored this relationship by computing, for
255 each individual brain state, the cosine similarity of the positive and negative activations of
256 the cluster's centroid with a set of a priori defined functional 'communities' or networks
257 (Schaefer et al., 2018; Yeo et al., 2011). The results were visualized as spider plots for the
258 Schaefer atlases.

259 In further exploratory analyses, we describe the associations between brain state dy-
260 namics and other measures of cognitive ability such as memory and language.

261 **Pilot data and analysis**

262 Summary data from the first 1000 imaging data points of the HCHS have been published
263 with (Schlemm et al., 2022) and formed the basis for the hypotheses tested in this replication
264 study. Before pre-registration, we had implemented our prespecified analysis pipeline described
265 above in R and Matlab, and applied it to this previous sample. Data, code and results

266 [from this pilot analysis have been stored with the archived Stage 1 report on GitHub](#)
267 [\(https://github.com/csi-hamburg/HCHS_brain_states_RR_v1.5\)](https://github.com/csi-hamburg/HCHS_brain_states_RR_v1.5) and preserved on Zenodo.

268 **Timeline and access to data**

269 [At the time of planning of this study, all demographic, clinical and imaging data used in](#)
270 [this analysis had been collected by the HCHS and were held in the central trial database.](#)
271 [Quality checks for non-imaging variables had been performed centrally. WMH segmentation](#)
272 [based on structural MRI data of the first 10 000 participants of the HCHS had been performed](#)
273 [previously using the BIANCA/LOCATE approach \(Rimmele et al., 2022\). Functional MRI](#)
274 [data and clinical measures of executive dysfunction \(TMT-B scores\) had not previously](#)
275 [been analyzed by the pre-registering author \(ES\).](#)

276 **Deviations from preregistration**

277 For deconfounding and aggregating BOLD data at brain parcellation level, the software
278 xcpEngine was used in version 1.2.3, not 1.2.1, to ensure that that the correct MNI ref-
279 erence template (MNI152Nlin2009cAsym) is used for registration of brain atlases. This
280 decision was made before analysing the data.

281 **Results**

282 For this replication study, a total of 2648 datasets were available, of which 970 were al-
283 ready included in our previous analysis and thus discarded. In 13 of the resulting 1678
284 datasets, one or more MRI sequences were missing. Of the complete datasets (n=1665),
285 we excluded 5 participants due to intra-axial space-occupying lesions. An additional 9
286 ~~subjects~~ [participants](#) were excluded because of unsuccessful preprocessing, WMH seg-
287 mentation, or xcpEngine failure, resulting in 1651 datasets for analysis. A study-flowchart
288 is provided in Figure 2.

289 Baseline demographic and cognitive values, including the number of missing items,
290 are reported in Table 4.

291 WMH volumes (median 1.05 mL, IQR 0.47 mL to 2.37 mL), motion estimates, and frac-
292 tional occupancies of brain states 1 through 5 are reported in Table 5.

293 In an outcome-neutral quality check of the implementation of (i) the MRI processing
294 pipeline, (ii) brain state estimation, and (iii) co-activation pattern analysis, the mean differ-
295 ence in fractional occupancy between high- and low-occupancy states was consistently

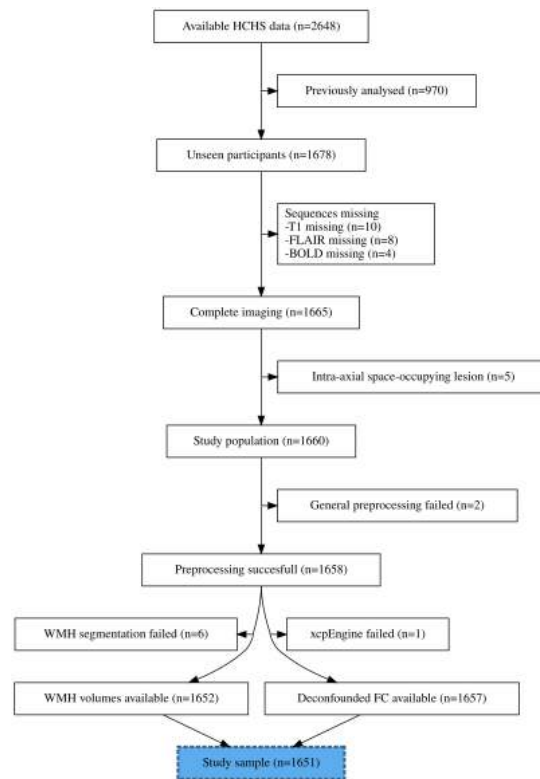


Figure 2 | Study flowchart. Composition of the study population after application of inclusion and exclusion criteria, and image processing.

296 maintained, with a point-estimate of the separation between two high-occupancy and
 297 three low-occupancy states of 6.7 % (95 % confidence interval, 6.2 % to 7.1 %) in the 36p
 298 paradigm. This indicates that the implementation of the pipeline was correct and that
 299 the brain state estimation and co-activation pattern analysis worked as intended.

300 Pre-registered hypotheses

301 Association between WMH load and fractional occupancy

302 The results of the test of our primary preregistered hypothesis of an association be-
 303 tween supratentorial WMH volume and the time spent in high-occupancy brain states
 304 are shown in Figure 3 and Table 7.

305 Adjusted for age and sex, there was a 0.94-fold reduction in the odds of occupying a
 306 high-occupancy brain state for every 5.1-fold increase in WMH load ($P 5.01 \times 10^{-8}$).

307 Association between executive function and fractional occupancy in DMN- 308 related states

309 The results of the test of our secondary preregistered hypothesis of an association be-
 310 tween time spent in high-occupancy brain states and executive function as measured by

the complete part B of the TMT are shown in Figure 4 and Table 9.

312 Adjusted for age, sex, WMH volume, and years of education, there was a 0.98-fold
 313 reduction in the time to complete the TMT-B for every 5 % increase in the time spent in

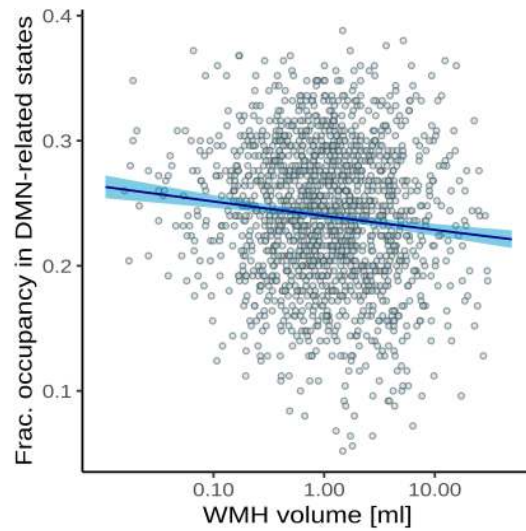


Figure 3 | Association between time spent in high-occupancy brain states and supratentorial WMH volume. Point estimates (black line) and 95%-confidence region (light blue ribbon) of the conditional mean fractional occupancy are obtained from unadjusted beta regression modelling. Each marker represents one of N=1642 independent participants with a non-zero total WMH volume.

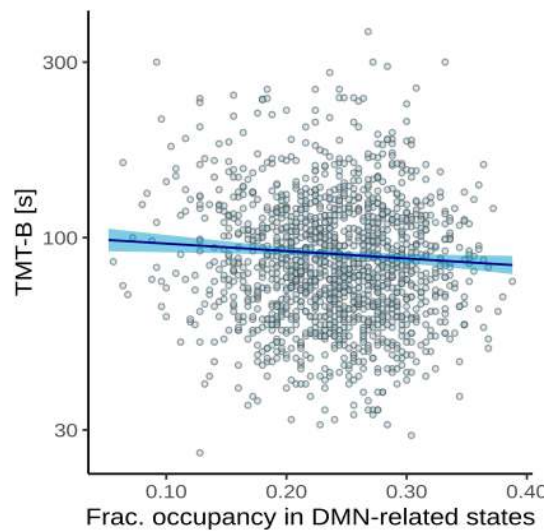


Figure 4 | Association between time spent in high-occupancy DMN-related brain states and TMT-B completion time. Point estimates (black line) and 95%-confidence region (light blue ribbon) of the conditional mean TMT-B completion time are obtained from unadjusted Gamma regression modelling. Each marker represent one of N=1482 independent participants with non-zero total WMH volume and available TMT-B data.

327 icant negative and no significant positive associations, irrespective of operationalization
328 of cSVD (total vs. periventricular vs. deep WMH volume) (Figure 5B).

329 **Additional analyses**

330 Connectivity profiles of brain states – relation to default mode network
331 Based on the cosine similarity between positive and negative activations of cluster cen-
332 troids and indicator vectors of pre-defined large scale brain networks, network activation
333 profiles were computed for brain states estimated from Schaefer parcellations of varying
334 spatial ~~resolution~~resolutions.

335 Figure 6 shows the corresponding spider plots, identifying states characterized by
336 activation (DMN+) or suppression (DMN-) of the default mode network as states with the
337 highest fractional occupancy.

338 Association with other cognitive domains

339 Associations between the time spent in high-occupancy DMN-related brain states and
340 cognitive measures beyond TMT-B are shown in Figure 7.

341 Adjusted for age, sex, WMH load, and years of education, FO in DMN-related states
342 appeared to be associated with better word recall (~~aOR~~adjusted OR 1.19, nominal P
343 0.013), but not with global cognitive functioning (MMSE, ~~aOR~~adjusted OR 1.09) or vocab-
344 ulary (aOR 1.09), nor with verbal fluency (animal naming, adjusted $\exp(\beta)$ 1.04), or pure
345 processing speed (TMT-A, adjusted $\exp(\beta)$ 0.97).

346 **Summary and Discussion**

347 In this pre-registered cross-sectional study we replicated the key findings of Schlemm
348 et al., 2022 in an independent population-based sample of 1651 middle-aged to elderly
349 participants of the Hamburg City Health Study.

350 First, we confirmed that the severity of cerebral small vessel disease is associated with
351 the time spent in high-occupancy brain states, defined by functional MRI. More precisely,
352 we showed that every 5.1-fold increase in the volume of supratentorial white matter hy-
353 perintensities of presumed vascular origin (WMH) was associated with a 0.95-fold reduc-
354 tion in the odds of occupying a brain state characterized by activation or suppression of
355 the default-mode network, at any given time during the resting-state scan.

356 Second, we confirmed that the time spent in high-occupancy brain states at rest is
357 associated with cognitive performance. More precisely, a 5%-reduction in the fractional

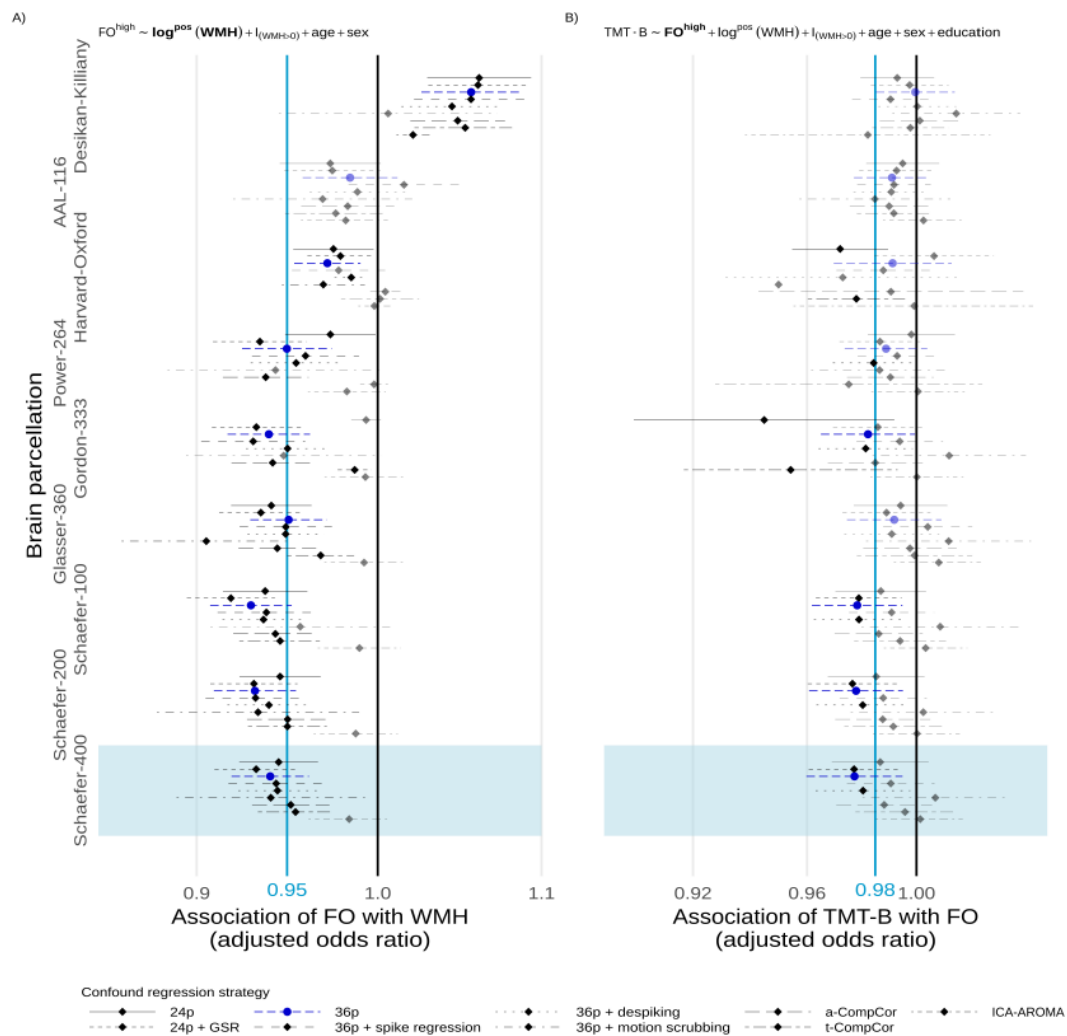


Figure 5 | Multiverse analysis. Adjusted effect size estimates of the associations between cSVD severity (WMH volume) and network dedifferentiation (less time spent in high-occupancy DMN-related brain states) [A], and between network dedifferentiation and executive function (TMT-B completion time) [B]. Effect sizes are given per 5.1-fold increase in WMH volume and a 5%-increase in fractional occupancy, respectively. Markers and line segments indicate point estimates and 95%-confidence intervals for adjusted odds ratios for different combinations of confound regression strategy and brain parcellation. The primary analytical choices are indicated by dark blue circles (36p) and light blue shading (Schaefer-400). Model equations for beta and gamma regressions, respectively, are given at the top. Vertical lines indicate no effect (black) and the effect size observed in the discovery cohort (Schlemm et al., 2022) (light blue), respectively, for reference. Effect sizes not reaching nominal statistical significance ($\alpha = 0.05$) are shown desaturated. Corresponding data based on periventricular and deep WMH volumes are presented in the Supplementary Appendix.

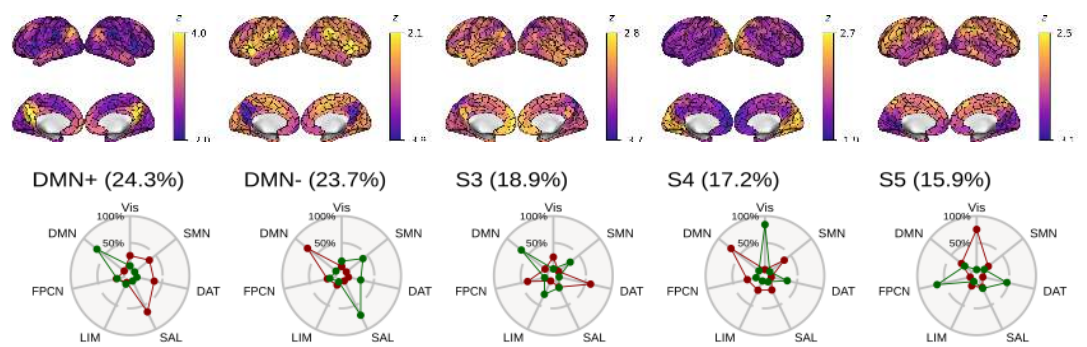


Figure 6 | Connectivity profiles of brain states. [Top] Centroids of each identified brain state visualized in brain space. Note the individual color scales. [Bottom] Cosine similarity between centroids of brain states and signed indicator vectors corresponding to activation (green) and suppression (red) of each of seven predefined large-scale functional brain networks (Yeo et al., 2011).

States are ordered by mean fractional occupancy across N=1651 independent participants, indicated by parenthetical percentages. Two high-occupancy states are characterized by activation or suppression of the DMN, the remaining three low-occupancy states (S3–5) were not used in the present study. Note that mean FO values are similar, but not identical, to median FO values reported in Table 5.

358 occupancy of DMN-related brain states was associated with a 1.02-fold increase in the
 359 time to complete part B of the trail making test (TMT).

360 In a pre-planned multiverse analysis, [these findings](#) [findings relating to our primary](#)
 361 [and, to a lesser extent, secondary hypotheses](#) were robust with respect to variations in
 362 brain parcellations and confound regression strategies. Inconsistent results were found
 363 with the Desikan–Killiany parcellation, likely reflecting the notion that the spatial resolu-
 364 tion and functional specificity of this coarse, structurally defined atlas are inadequate for
 365 analyzing functionally defined brain states. Across brain parcellations, effect sizes were
 366 smaller with the ICA-AROMA confound regression strategy and failed to reach nominal
 367 statistical significance. This might be due to a relatively large residual motion compo-
 368 nent in measures of dynamical functional Connectivity after de-noising with ICA-AROMA,
 369 as described previously (Lydon-Staley et al., 2019).

370 We also confirmed across several brain parcellation resolutions that high-occupancy
 371 states at rest are characterized by either activation or suppression of the default mode
 372 network, reflecting its role as the predominant task-negative brain network.

373 In unplanned, exploratory analyses, we described the association between brain state
 374 dynamics and cognitive measures other than executive function and processing speed
 375 and reported a strong, preliminary association between time spent in high-occupancy
 376 states and delayed word recall.

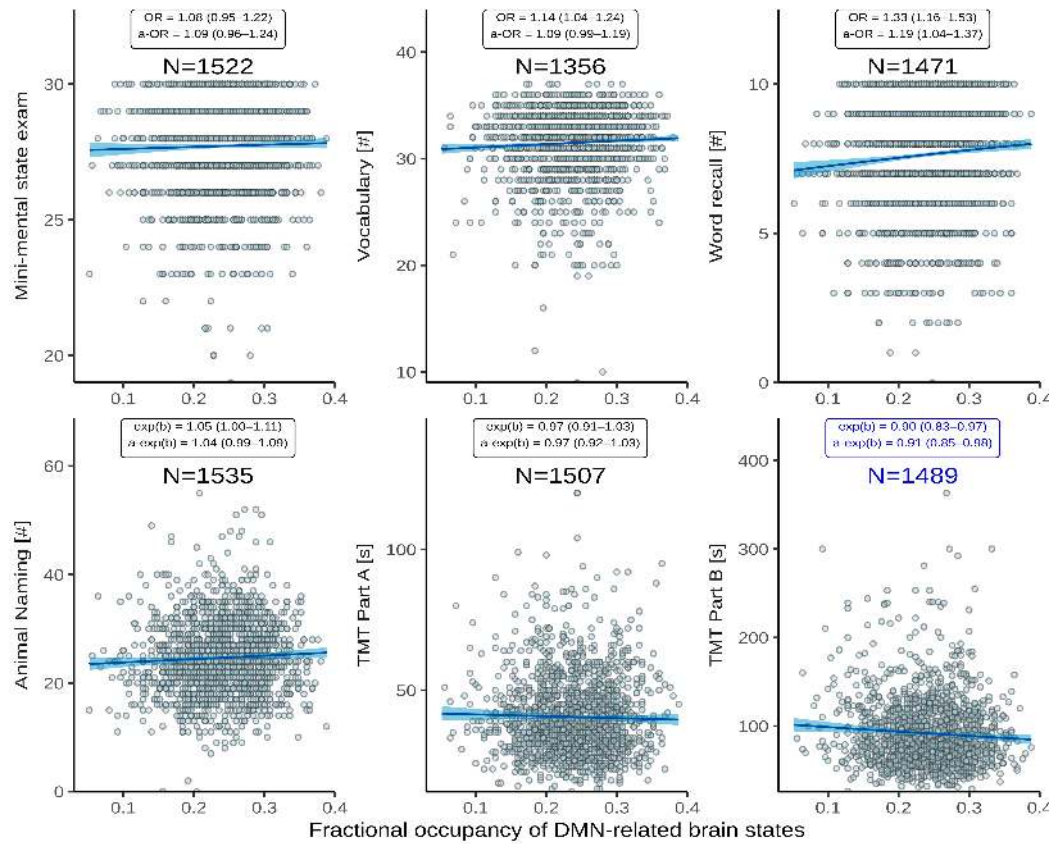


Figure 7 | Association between time spent in high-occupancy DMN-related brain states and cognitive measures. Point estimates (black line) and 95%-confidence region (light blue ribbon) of the conditional mean cognitive measures are obtained from unadjusted binomial (top row: Mini-Mental State Examination, Vocabulary, Word List Recall, logit link) and Gamma regression (bottom row: Animal Naming, Trail Making Test [TMT] A/B: log link) modelling. Each marker represents one of N independent participants, as indicated. Insets report effect sizes and P-values both with (adjusted [a-]) and without adjustment for the nuisance variables age, sex, WMH volume (coded as in Figure 5), and years of education. Effect sizes were quantified as odds ratios (ORs) (top) or response scale multipliers [exp(b)] (bottom), and correspond to a 20%-increase in fractional occupancy. Note the different reference change in FO compared to Table 9 chosen to adequately represent some of the smaller effect sizes. The bottom right panel highlighted in dark blue reproduces Figure 4.

377 We further explored, ~~but did not report in detail~~ and report in the Supplementary
378 appendix, the effect of motion; ~~all reported associations~~ results relating to our primary
379 and, to a lesser extent, secondary, hypotheses were robust to additional, unplanned ad-
380 justments for DVARS, RMSD ~~or,~~ and mean framewise displacement.


381 The presented results provide robust evidence for a behaviorally relevant association
382 between cerebral small vessel disease and functional brain network dedifferentiation.

383 Further research is required to replicate our findings in different populations, such
384 as those affected more severely by cSVD or cognitive impairment, or being studied using
385 different imaging protocols, to determine the generalizability of our findings with respect
386 to varying operationalizations of the notions of cSVD, brain state, and cognition, and to
387 understand the mechanisms underlying the reported associations.

388 **Timeline and access to data**

389 ~~At the time of planning of this study, all demographic, clinical and imaging data used in~~
390 ~~this analysis had been collected by the HCHS and were held in the central trial database.~~
391 ~~Quality checks for non-imaging variables had been performed centrally. WMH segmentation~~
392 ~~based on structural MRI data of the first 10 000 participants of the HCHS had been performed~~
393 ~~previously using the BIANCA/LOCATE approach. Functional MRI data and clinical measures~~
394 ~~of executive dysfunction (TMT-B scores) had not previously been analyzed by the pre-registering~~
395 ~~author (ES).~~

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397 This preprint was created using the LaPreprint template ([https://github.com/roaldarbol/](https://github.com/roaldarbol/lapreprint)
398 [lapreprint](https://github.com/roaldarbol/lapreprint)) by Mikkel Roald-Arbøl .

399 **Disclosure**

400 The authors of this article declare that they have no financial conflict of interest with the
401 content of this article.

402 **References**

403 Arbuthnott, Katherine and Janis Frank (2000). "Trail making test, part B as a measure of
404 executive control: validation using a set-switching paradigm". In: *Journal of clinical and*
405 *experimental neuropsychology* 22.4, pp. 518–528.

- 406 Behzadi, Yashar et al. (2007). "A component based noise correction method (CompCor)
407 for BOLD and perfusion based fMRI". In: *Neuroimage* 37.1, pp. 90–101.
- 408 Bos, Daniel et al. (2018). "Cerebral small vessel disease and the risk of dementia: A sys-
409 tematic review and meta-analysis of population-based evidence". en. In: *Alzheimers.*
410 *Dement.* 14.11, pp. 1482–1492.
- 411 Cannistraro, Rocco J et al. (2019). "CNS small vessel disease: A clinical review". en. In: *Neu-*
412 *rology* 92.24, pp. 1146–1156.
- 413 Ciric, Rastko, Adon FG Rosen, et al. (2018). "Mitigating head motion artifact in functional
414 connectivity MRI". In: *Nature protocols* 13.12, pp. 2801–2826.
- 415 Ciric, Rastko, Daniel H Wolf, et al. (2017). "Benchmarking of participant-level confound
416 regression strategies for the control of motion artifact in studies of functional con-
417 nectivity". en. In: *Neuroimage* 154, pp. 174–187.
- 418 Cornblath, Eli J et al. (2020). "Temporal sequences of brain activity at rest are constrained
419 by white matter structure and modulated by cognitive demands". en. In: *Commun Biol*
420 3.1, p. 261.
- 421 Cox, Robert W (1996). "AFNI: software for analysis and visualization of functional mag-
422 netic resonance neuroimages". In: *Computers and Biomedical research* 29.3, pp. 162–
423 173.
- 424 Das, Alvin S et al. (2019). "Asymptomatic Cerebral Small Vessel Disease: Insights from
425 Population-Based Studies". en. In: *J. Stroke Cerebrovasc. Dis.* 21.2, pp. 121–138.
- 426 Desikan, Rahul S et al. (2006). "An automated labeling system for subdividing the human
427 cerebral cortex on MRI scans into gyral based regions of interest". In: *Neuroimage* 31.3,
428 pp. 968–980.
- 429 Dey, Ayan K et al. (2016). "Pathoconnectomics of cognitive impairment in small vessel
430 disease: A systematic review". en. In: *Alzheimers. Dement.* 12.7, pp. 831–845.
- 431 Esteban, Oscar et al. (2019). "fMRIPrep: a robust preprocessing pipeline for functional
432 MRI". en. In: *Nat. Methods* 16.1, pp. 111–116.
- 433 Frey, Benedikt M et al. (2021). "White matter integrity and structural brain network topol-
434 ogy in cerebral small vessel disease: The Hamburg city health study". en. In: *Hum. Brain*
435 *Mapp.* 42.5, pp. 1406–1415.
- 436 Friston, Karl J et al. (1996). "Movement-related effects in fMRI time-series". In: *Magnetic*
437 *resonance in medicine* 35.3, pp. 346–355.

438 Gesierich, Benno et al. (2020). "Alterations and test-retest reliability of functional connec-
439 tivity network measures in cerebral small vessel disease". en. In: *Hum. Brain Mapp.*
440 41.10, pp. 2629–2641.

441 Glasser, Matthew F et al. (2016). "A multi-modal parcellation of human cerebral cortex".
442 en. In: *Nature* 536.7615, pp. 171–178.

443 Gordon, Evan M et al. (2016). "Generation and Evaluation of a Cortical Area Parcellation
444 from Resting-State Correlations". en. In: *Cereb. Cortex* 26.1, pp. 288–303.

445 Griffanti, Ludovica, Mark Jenkinson, et al. (2018). "Classification and characterization of
446 periventricular and deep white matter hyperintensities on MRI: A study in older adults".
447 en. In: *Neuroimage* 170, pp. 174–181.

448 Griffanti, Ludovica, Giovanna Zamboni, et al. (2016). "BIANCA (Brain Intensity AbNormal-
449 ity Classification Algorithm): A new tool for automated segmentation of white matter
450 hyperintensities". en. In: *Neuroimage* 141, pp. 191–205.

451 Jagodzinski, Annika et al. (2020). "Rationale and Design of the Hamburg City Health Study".
452 en. In: *Eur. J. Epidemiol.* 35.2, pp. 169–181.

453 Laumann, Timothy O, Evan M Gordon, et al. (2015). "Functional system and areal organi-
454 zation of a highly sampled individual human brain". In: *Neuron* 87.3, pp. 657–670.

455 Laumann, Timothy O and Abraham Z Snyder (2021). "Brain activity is not only for thinking".
456 In: *Current Opinion in Behavioral Sciences* 40, pp. 130–136.

457 Laumann, Timothy O, Abraham Z Snyder, et al. (2017). "On the stability of BOLD fMRI
458 correlations". In: *Cerebral cortex* 27.10, pp. 4719–4732.

459 Lawrence, Andrew J, Ai Wern Chung, et al. (2014). "Structural network efficiency is as-
460 sociated with cognitive impairment in small-vessel disease". en. In: *Neurology* 83.4,
461 pp. 304–311.

462 Lawrence, Andrew J, Daniel J Tozer, et al. (2018). "A comparison of functional and trac-
463 tography based networks in cerebral small vessel disease". en. In: *Neuroimage Clin* 18,
464 pp. 425–432.

465 Lawrence, Andrew J, Eva A Zeestraten, et al. (2018). "Longitudinal decline in structural
466 networks predicts dementia in cerebral small vessel disease". en. In: *Neurology* 90.21,
467 e1898–e1910.

468 Lydon-Staley, David M et al. (2019). "Evaluation of confound regression strategies for
469 the mitigation of micromovement artifact in studies of dynamic resting-state func-

470 tional connectivity and multilayer network modularity". In: *Network Neuroscience* 3.2,
471 pp. 427–454.

472 Macey, Paul M et al. (2004). "A method for removal of global effects from fMRI time series".
473 In: *Neuroimage* 22.1, pp. 360–366.

474 Makris, Nikos et al. (2006). "Decreased volume of left and total anterior insular lobule in
475 schizophrenia". In: *Schizophrenia research* 83.2-3, pp. 155–171.

476 Muschelli, John et al. (2014). "Reduction of motion-related artifacts in resting state fMRI
477 using aCompCor". In: *Neuroimage* 96, pp. 22–35.

478 Petersen, Marvin et al. (2020). "Network Localisation of White Matter Damage in Cerebral
479 Small Vessel Disease". en. In: *Sci. Rep.* 10.1, p. 9210.

480 Power, Jonathan D, Alexander L Cohen, et al. (2011). "Functional network organization of
481 the human brain". en. In: *Neuron* 72.4, pp. 665–678.

482 Power, Jonathan D, Anish Mitra, et al. (2014). "Methods to detect, characterize, and re-
483 move motion artifact in resting state fMRI". In: *Neuroimage* 84, pp. 320–341.

484 Prins, Niels D et al. (2005). "Cerebral small-vessel disease and decline in information pro-
485 cessing speed, executive function and memory". en. In: *Brain* 128.Pt 9, pp. 2034–2041.

486 Pruijm, Raimon HR et al. (2015). "ICA-AROMA: A robust ICA-based strategy for removing
487 motion artifacts from fMRI data". In: *Neuroimage* 112, pp. 267–277.

488 Reijmer, Yael D et al. (2016). "Small vessel disease and cognitive impairment: The rele-
489 vance of central network connections". en. In: *Hum. Brain Mapp.* 37.7, pp. 2446–2454.

490 Rimmele, David Leander et al. (2022). "Association of Carotid Plaque and Flow Velocity
491 With White Matter Integrity in a Middle-aged to Elderly Population". en. In: *Neurology*.

492 Satterthwaite, Theodore D et al. (2013). "An improved framework for confound regres-
493 sion and filtering for control of motion artifact in the preprocessing of resting-state
494 functional connectivity data". In: *Neuroimage* 64, pp. 240–256.

495 Schaefer, Alexander et al. (2018). "Local-Global Parcellation of the Human Cerebral Cortex
496 from Intrinsic Functional Connectivity MRI". en. In: *Cereb. Cortex* 28.9, pp. 3095–3114.

497 Schlemm, Eckhard et al. (2022). "Equalization of Brain State Occupancy Accompanies
498 Cognitive Impairment in Cerebral Small Vessel Disease". en. In: *Biol. Psychiatry* 92.7,
499 pp. 592–602.

500 Schulz, Maximilian et al. (2021). "Functional connectivity changes in cerebral small vessel
501 disease - a systematic review of the resting-state MRI literature". en. In: *BMC Med.* 19.1,
502 p. 103.

- 503 Shen, Jun et al. (2020). "Network Efficiency Mediates the Relationship Between Vascular
504 Burden and Cognitive Impairment: A Diffusion Tensor Imaging Study in UK Biobank".
505 en. In: *Stroke* 51.6, pp. 1682–1689.
- 506 Steegen, Sara et al. (2016). "Increasing Transparency Through a Multiverse Analysis". en.
507 In: *Perspect. Psychol. Sci.* 11.5, pp. 702–712.
- 508 Sundaresan, Vaanathi et al. (2019). "Automated lesion segmentation with BIANCA: Im-
509 pact of population-level features, classification algorithm and locally adaptive thresh-
510 olding". en. In: *Neuroimage* 202, p. 116056.
- 511 Tombaugh, Tom N (2004). "Trail Making Test A and B: normative data stratified by age
512 and education". en. In: *Arch. Clin. Neuropsychol.* 19.2, pp. 203–214.
- 513 Tuladhar, Anil M, Ewoud van Dijk, et al. (2016). "Structural network connectivity and cog-
514 nition in cerebral small vessel disease". en. In: *Hum. Brain Mapp.* 37.1, pp. 300–310.
- 515 Tuladhar, Anil M, Jonathan Tay, et al. (2020). "Structural network changes in cerebral small
516 vessel disease". en. In: *J. Neurol. Neurosurg. Psychiatry* 91.2, pp. 196–203.
- 517 Tzourio-Mazoyer, Nathalie et al. (2002). "Automated anatomical labeling of activations in
518 SPM using a macroscopic anatomical parcellation of the MNI MRI single-subject brain".
519 In: *Neuroimage* 15.1, pp. 273–289.
- 520 Vidaurre, Diego et al. (2018). "Discovering dynamic brain networks from big data in rest
521 and task". en. In: *Neuroimage* 180.Pt B, pp. 646–656.
- 522 Wardlaw, Joanna M, Colin Smith, and Martin Dichgans (2013). "Mechanisms of sporadic
523 cerebral small vessel disease: insights from neuroimaging". en. In: *Lancet Neurol.* 12.5,
524 pp. 483–497.
- 525 Wardlaw, Joanna M, Eric E Smith, et al. (2013). "Neuroimaging standards for research
526 into small vessel disease and its contribution to ageing and neurodegeneration". en.
527 In: *Lancet Neurol.* 12.8, pp. 822–838.
- 528 Wardlaw, Joanna M, Maria C Valdés Hernández, and Susana Muñoz-Maniega (2015). "What
529 are white matter hyperintensities made of? Relevance to vascular cognitive impair-
530 ment". en. In: *J. Am. Heart Assoc.* 4.6, p. 001140.
- 531 Xu, Yuanhang et al. (2021). "Altered Dynamic Functional Connectivity in Subcortical Is-
532 chemic Vascular Disease With Cognitive Impairment". en. In: *Front. Aging Neurosci.* 13,
533 p. 758137.
- 534 Yeo, B T Thomas et al. (2011). "The organization of the human cerebral cortex estimated
535 by intrinsic functional connectivity". en. In: *J. Neurophysiol.* 106.3, pp. 1125–1165.

536 Yin, Wenwen et al. (2022). "The Clustering Analysis of Time Properties in Patients With
537 Cerebral Small Vessel Disease: A Dynamic Connectivity Study". en. In: *Front. Neurol.*
538 13, p. 913241.

Question	Hypothesis	Sampling plan	Analysis plan	Ratio- rate for decid- ing the sensi- tivity of the test	Interpretation given different outcomes	Theory that could be shown wrong by the outcome
Is severity of cerebral small disease, quantified by the volume of supratentorial white matter hyperintensities of presumed vascular origin (WMH), associated with time spent in high-occupancy brain states, defined by resting-state functional MRI?	(Primary) Higher WMH volume is associated with lower average occupancy of the two highest-occupancy brain states.	Available subjects participants with clinical and imaging data from the the HCHS (Jagodzinski et al., 2020)	Standardized preprocessing of structural and functional MRI data • automatic quantification of WMH • co-activation pattern analysis • multivariable generalised regression analyses	Tradition	$P < 0.05$ → rejection of the null hypothesis of no association between cSVD and fractional occupancy; $P > 0.05$ → insufficient evidence to reject the null hypothesis	Functional brain dynamics are not related to subcortical ischemic vascular disease.
Is time spent in high-occupancy brain states associated with cognitive impairment, measured as the time to complete part B of the trail making test (TMT)?	(Secondary) Lower average occupancy of the two highest-occupancy brain states is associated with longer TMT-B time.	as above	as above	as above	$P < 0.05$ → rejection of the null hypothesis of no association between fractional occupancy and cognitive impairment; $P > 0.05$ → insufficient evidence to reject the null hypothesis	Cognitive function is not related to MRI-derived functional brain dynamics.

Table 1 | Study Design Template. Overview of the Scientific Questions addressed in the present study (first column), the two main hypotheses being investigated (second column), and details of the underlying study.

Name of the atlas	#parcels	Reference
Desikan–Killiany	86	Desikan et al., 2006
AAL	116	Tzourio-Mazoyer et al., 2002
Harvard–Oxford	112	Makris et al., 2006
glasser360	360	Glasser et al., 2016
gordon333	333	Gordon et al., 2016
power264	264	Power, Cohen, et al., 2011
schaefer{N}	100	Schaefer et al., 2018
	200	
	400	

AAL: Automatic Anatomical Labelling

(a) Parcellations

Design	Reference
24p	Friston et al., 1996
24p + GSR	Macey et al., 2004
36p	Satterthwaite et al., 2013
36p + spike regression	Cox, 1996
36p + despiking	Satterthwaite et al., 2013
36p + scrubbing	Power, Mitra, et al., 2014
aCompCor	Muschelli et al., 2014
tCompCor	Behzadi et al., 2007
AROMA	Pruim et al., 2015

GSR: Global signal regression, AROMA: Automatic Removal of Motion Artifacts

(b) Confound regression strategies, adapted from (Circic, Wolf, et al., 2017)

Table 2 | Multiverse analysis. Overview over different brain parcellations and confound regression strategies implemented using xcpEngine (Circic, Rosen, et al., 2018). A total of $9 \times 9 = 81$ analytical combinations were explored to assess the robustness of our results with respect to these processing choices.

N = 1,651	
<i>Demographics (no Missing n (%))</i>	
Age, yr	
Median (IQR)	66 (59 – 72)
Sex	
Male	940/1651 (57%)
Female	711/1651 (43%)
<i>Cardiovascular risk factors</i>	
Hypertension	
Present	1177/1611 (73.1%)
Missing n (%)	85 (5.1%)
Diabetes	
Present	157/1566 (10%)
Missing n (%)	40 (2.4%)
Smoking	
Present	200/1360 (14.7%)
Missing n (%)	201 (12.9%%)
Hyperlipidaemia	
Present	426/1578 (27%)
Missing n (%)	73 (4.4%)
<i>Cognitive test results</i>	
MMSE, # (max. 30)	
Median (IQR)	28 (27 – 29)
Missing n (%)	129 (7.8%)
Vocabulary (MWT-B), # (max. 37)	
Median (IQR)	32 (30 – 34)
Missing n (%)	295 (18%)
Word recall, # (max. 10)	
Median (IQR)	8 (6 – 9)
Missing n (%)	180 (11%)
Animal Naming	
Median (IQR)	24 (20 – 29)
Missing n (%)	116 (7.0%)
TMT-A, seconds	
Median (IQR)	38 (31 – 48)
Missing n (%)	144 (8.7%)
TMT-B, seconds	
Median (IQR)	83 (65 – 110)
Missing n (%)	162 (9.8%)
<i>History</i>	
Diagnosed dementia	
Present	6/1645 (0.4%)
Missing n (%)	6 (0.4%)
Years of education	
Median (IQR)	13 (12 – 16)
Missing n (%)	34 (2%)

Table 4 | Descriptive statistics of the study population. Data are presented as median (interquartile range) or count (percentage) of non-missing items, as appropriate. Number of percentage of missing items are reported separately.

N = 1,651	
WMH volume ¹ , mL	
Total	1.05 (0.47 – 2.37), 9 Z
Periventricular	0.94 (0.43 – 2.04), 9 Z
Deep	0.10 (0.03 – 0.37), 344 Z
Motion during rs-fMRI	
Frame-wise displacement, mm	0.21 (0.15 – 0.63)
RMSD, mm	0.086 (0.058 – 0.12)
DVARs	27.8 (24.3 – 31.8)
Fractional occupancy, %	
DMN+	24.8 (20.8 – 28.0)
DMN-	24.0 (20.0 – 28.0)
S3	18.4 (15.2 – 22.4)
S4	16.8 (12.8 – 20.8)
S5	15.2 (12.0 – 19.2)

¹Number of zero values indicated by Z

Table 5 | Structural and functional imaging characteristics. Data are presented as median (interquartile range). Supratentorial WMH volumes were obtained by semiautomatic segmentation of FLAIR images using a BINACA/LOCATE-based *k*-nearest neighbours algorithm and stratified by their distance to the lateral ventricles (<10 mm, periventricular; >10 mm, deep). Motion parameters were estimated during fMRIprep processing of BOLD scans. Fractional occupancies were calculated by assigning individual BOLD volumes to one of five discrete brain states defined by *k*-means clustering-based co-activation pattern analysis. Two high-occupancy states are labelled DMN+ and DMN- in view of their network connectivity profiles as shown in Figure 6.

	Estimate	P	95%-CI
Intercept	0.24	<0.0001	0.21 – 0.27
WMH, per 5.1-fold increase ¹	0.94	<0.0001	0.92 – 0.96
Age, per 10 years	1.04	0.001	1.01 – 1.06
Female sex	1.12	<0.0001	1.09 – 1.16
$\mathbf{1}_{\{WMH=0\}}$	0.93	0.477	0.75 – 1.14

¹ Interquartile ratio 2.37/0.468 = 5.06

Table 7 | Association between time-spent in high-occupancy DMN-related brain states and WMH volume adjusted for age and sex. Beta regression table estimated from $n = 1651$ independent participants using the model equation $FO^{high} \sim \log WMH^+ + \mathbf{1}_{\{WMH=0\}} + age + sex$.

	Estimate	P	95%-CI
Intercept	53.41	< 0.0001	42.7 – 66.8
FO ^{high} , per 5%	0.98	0.0116	0.96 – 0.99
WMH, per 5.1-fold increase ¹	1.01	0.367	0.98 – 1.05
Age, per 10 years	1.18	<0.0001	1.15 – 1.21
Female sex	0.99	0.666	0.95 – 1.03
Education, per year	0.97	<0.0001	0.97 – 0.98
$\mathbf{1}_{\{WMH=0\}}$	0.97	0.398	0.92 – 1.03

¹ Interquartile ratio 2.37/0.468 = 5.06

Table 9 | Association between TMT-B and time spent in high-occupancy DMN-related brain states adjusted for age, sex, WMH volume and years of education. Gamma regression table

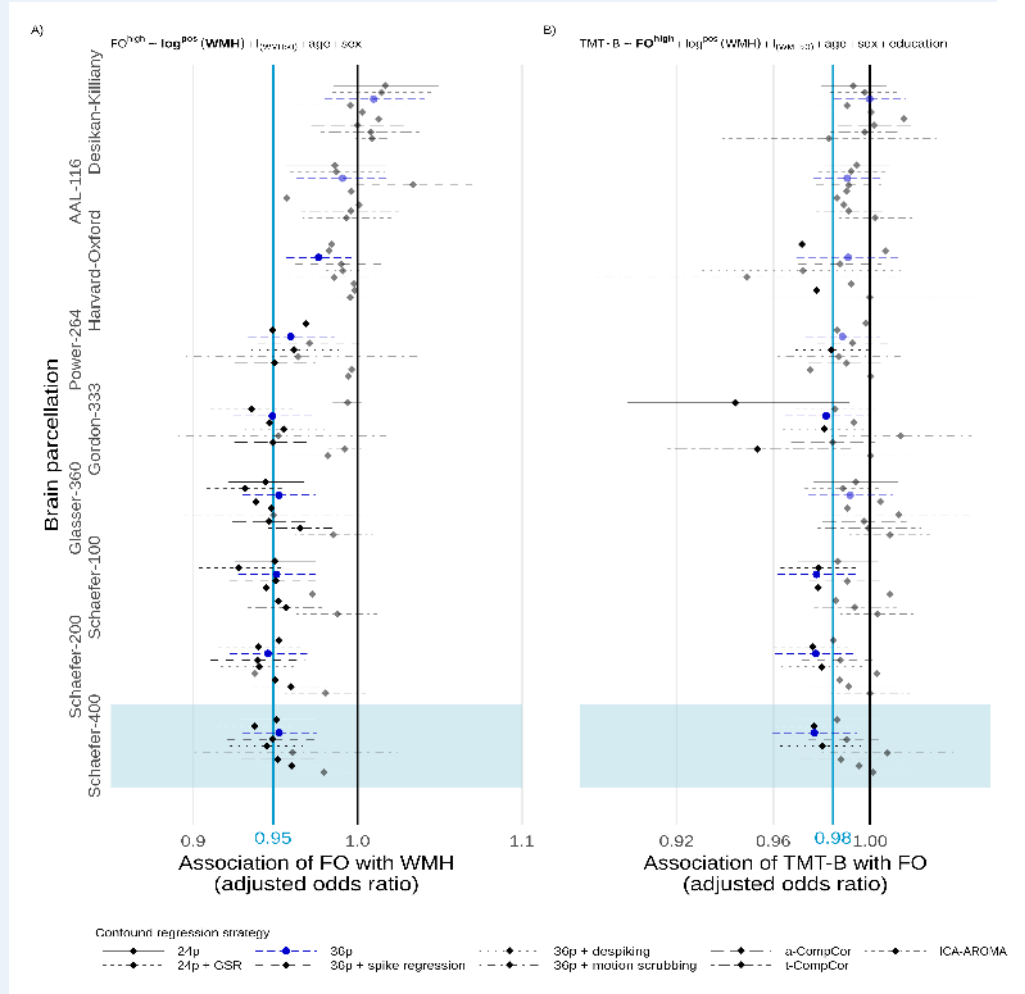
estimated from $n = 1483$ independent participants using the model equation

$TMT-B \sim FO^{high} + \log WMH^+ + \mathbf{1}_{\{WMH=0\}} + age + sex + educationyears.$

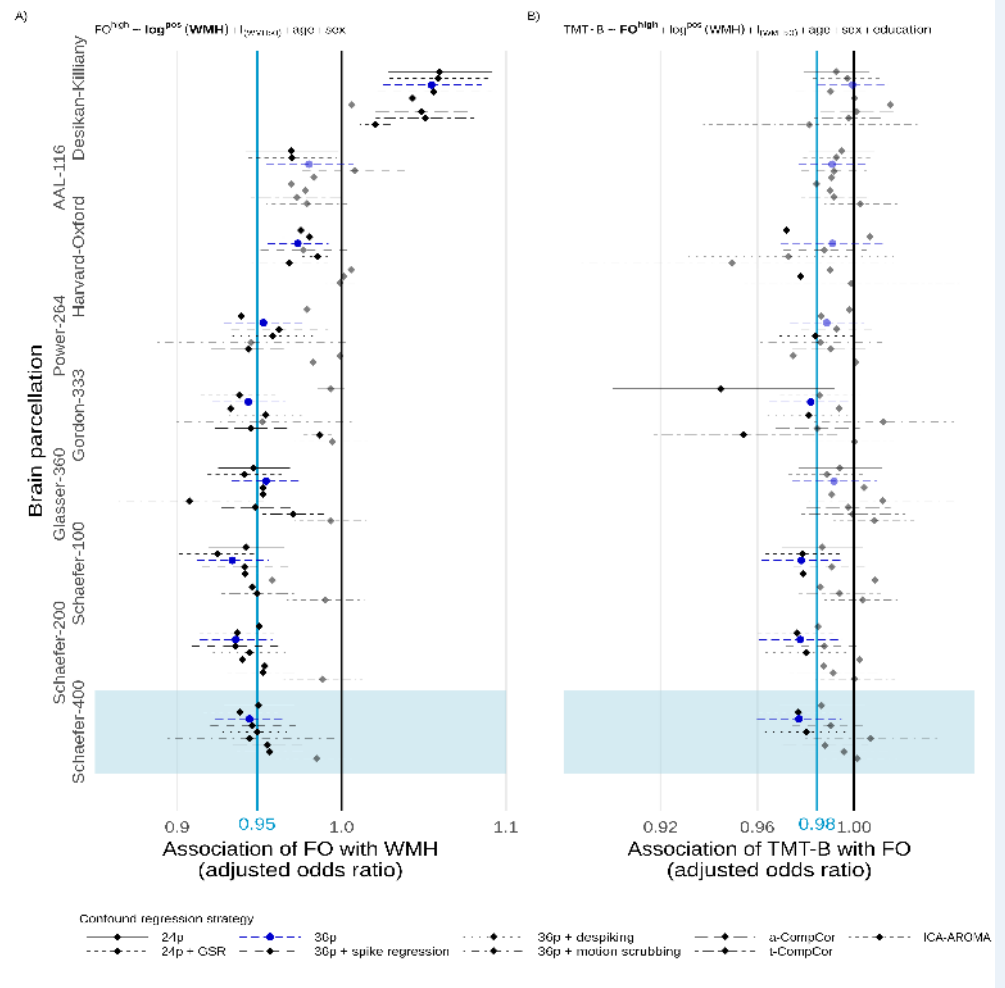
540 **Supplementary results**

541 **Deep and periventricular WMH**

542 Here we present, in analogy to Figure 5, the results of the multiverse analyses of
 543 the association between cSVD burden, FO of DMN-related states, and executive
 544 function, when cSVD is operationalized as the volume of deep or periventricular
 545 white matter hyperintensities, respectively.



546
548 **Appendix 1—figure 1 Multiverse analysis, deep WMH**



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Appendix 1—figure 2 Multiverse analysis, periventricular WMH

Motion parameters

We also present, in analogy to Tables 7 and 9, regression tables for the association between time spent in DMN-related brain states (FO) and WMH volume, and between TMT-B and FO, adjusted for DVARS, RSMD and framewise displacement, in addition to age, sex and, in the latter case, years of education.

	Estimate	P	95%-CI
Intercept	0.32	<0.0001	0.28 - 0.36
WMH, per 5.1-fold increase ¹	0.96	0.0004	0.94 - 0.98
Age, per 10 years	1.01	<0.0001	1.00 - 1.01
Female sex	1.11	<0.0001	1.08 - 1.15
$1_{\{WMH=0\}}$	0.91	0.3552	0.74 - 1.11

<u>DVARs</u>	<u>0.98</u>	<u><0.0001</u>	<u>0.98 – 0.99</u>
<u>RMSD</u>	<u>28.29</u>	<u>0.0055</u>	<u>2.67 – 299.84</u>
<u>Framewise displacement</u>	<u>0.16</u>	<u>0.0112</u>	<u>0.04 – 0.66</u>

¹ Interquartile ratio $2.37/0.468 = 5.06$

Appendix 1—table 2 Association between time-spent in high-occupancy DMN-related brain states and WMH volume adjusted for age, sex, and **motion parameters**

	<u>Estimate</u>	<u>P</u>	<u>95%-CI</u>
<u>Intercept</u>	<u>46.83</u>	<u><0.0001</u>	<u>36.74 – 59.72</u>
<u>FO^{high}, per 5%</u>	<u>0.71</u>	<u>0.0718</u>	<u>0.49 – 1.03</u>
<u>WMH, per 5.1-fold increase¹</u>	<u>1.01</u>	<u>0.3414</u>	<u>0.98 – 1.04</u>
<u>Age, per 10 years</u>	<u>1.02</u>	<u><0.0001</u>	<u>1.01 – 1.02</u>
<u>Female sex</u>	<u>1.00</u>	<u>0.8171</u>	<u>0.96 – 1.04</u>
<u>Education, per year</u>	<u>0.97</u>	<u><0.0001</u>	<u>0.97 – 0.98</u>
<u>1_(WMH=0)</u>	<u>0.96</u>	<u>0.7581</u>	<u>0.73 – 1.29</u>
<u>DVARs</u>	<u>1.01</u>	<u>0.0001</u>	<u>1.00 – 1.01</u>
<u>RMSD</u>	<u>0.31</u>	<u>0.4695</u>	<u>0.01 – 7.45</u>
<u>Framewise displacement</u>	<u>1.08</u>	<u>0.9322</u>	<u>0.16 – 7.13</u>

¹ Interquartile ratio $2.37/0.468 = 5.06$

Appendix 1—table 4 Association between TMT-B and time spent in high-occupancy DMN-related brain states adjusted for age, sex, WMH volume and years of education, and **motion parameters**

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